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## 1 Effective transcranial direct current stimulation (tDCS) parameters for the modulation

## 2 of eating behavior: A systematic literature review and meta-analysis

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- 6 Jordan D. Beaumont MMedSci<sup>a,\*</sup>, Natalie C. Smith<sup>a</sup>, David Starr BSc<sup>a</sup>, Danielle Davis PhD<sup>a</sup>,
- 7 Michelle Dalton PhD<sup>a</sup>, Alexander Nowicky PhD<sup>b</sup>, Mark Russell PhD<sup>a</sup> and Martin J. Barwood
- 8 PhD<sup>a</sup>
- 9
- 10 <sup>a</sup>School of Social and Health Sciences, Leeds Trinity University, Leeds, LS18 5HD, UK
- 11 <sup>b</sup>Centre for Cognitive Neuroscience, Department of Clinical Sciences, College of Health and
- 12 Life Sciences, Brunel University London, Uxbridge, UB8 3PH, UK
- 13
- 14 \* Corresponding author:
- 15 Jordan D. Beaumont
- 16 School of Social and Health Sciences, Leeds Trinity University, Leeds, LS18 5HD, UK
- 17 Email: j.beaumont@leedstrinity.ac.uk
- 18
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25 ABSTRACT

26 Objective

To consider the effect of differing transcranial direct current stimulation (tDCS) parameters
on eating-related measures, and how issues with experimental design (e.g., inadequate
blinding) or parameters variation may drive equivocal effects.

- 30
- 31 Methods

Literature searches were conducted across MEDLINE, PsycINFO, Scopus, and Science Direct. Studies using conventional sham-controlled tDCS to modify eating-related measures in adult human participants were included. A total of 1,135 articles were identified and screened by two independent authors. Study quality was assessed using the Risk of Bias tool. Random-effect meta-analyses were performed, with subgroup analyses to determine differences between parameter sets.

38

#### 39 Results

40 We identified 28 eligible studies; seven showed low risk of bias, with the remaining studies 41 showing bias arising from issues implementing or reporting blinding protocols. Large 42 variation in applied parameters was found, including montage, current intensity and density, 43 participant and researcher blinding, and the use of online or offline tasks. The application of 44 differing parameters appeared to alter the effects of tDCS on eating-related measures, 45 particularly for current density (g = -0.25 to 0.31), and when comparing single-session (g = -46 0.08 to 0.01) versus multi-session protocols (g = -0.34 to -0.29). Some parameters result in 47 null effects.

48

#### 49 Conclusion

The absence of tDCS-mediated change in eating-related measures may be driven by
 variation in applied parameters. Consistent application of parameters which appear effective

52 for modulating eating behavior is important for identifying the potential impact of tDCS. Using

53 the findings of this review, we propose a series of parameters that researchers should apply

54 in their work.

55

## 56 KEYWORDS

57 Appetite, Food consumption, Food craving, Food reward, Neuromodulation, Non-invasive

- 58 brain stimulation
- 59

## 60 ACRONYMS

- 61 CI = confidence interval; cm = centimeter; COMT = catechol-o-methyl transferase; DLPFC =
- 62 dorsolateral prefrontal cortex; EBA = extrastriate body area; g = Hedges' g; IFG = inferior
- 63 frontal gyrus; mA = milliampere; NIBS = non-invasive brain stimulation; PFC = prefrontal
- 64 cortex; PICO = Population, Intervention, Control and Outcome; PRISMA = Preferred
- 65 Reporting Items for Systematic Reviews and Meta-Analyses; RoB = risk of bias; SD =
- standard deviation; SE = standard error; tDCS = transcranial direct current stimulation; tnM1
- 67 = tongue muscle representation of the primary motor cortex

#### 69 **1. INTRODUCTION**

70 Over the last decade there has been increasing interest in the use of non-invasive brain 71 stimulation (NIBS) techniques, particularly transcranial direct current stimulation (tDCS), for 72 modifying eating behaviors associated with overconsumption and weight gain. Through 73 tDCS, a constant weak electrical current is applied to the brain via electrodes connected to a 74 battery-powered device (1, 2). Although the current strength is not sufficient to cause 75 neuronal firing, it appears able to modulate resting membrane potentials in a polarity-76 dependent manner through inhibition of neurotransmitters such as gamma-aminobutyric acid 77 and glutamate (3, 4). The electric current is delivered through an anode (positive charge) 78 electrode, where it is passed through the brain to a cathode (negative charge) electrode and 79 is returned to the device. In a simplistic view, the anode is associated with depolarization of 80 cortical activity and an increased likelihood of spontaneous neuronal firing. Conversely, the cathode is associated with hyperpolarization of the cortex resulting in the decreased 81 82 likelihood of spontaneous neuronal firing (3).

83

84 The ability of tDCS to alter eating behaviors, such as food craving and consumption, has 85 been of great interest for researchers due to its potential use in the treatment of obesity (5). 86 Since the first study using tDCS to alter food craving was published over a decade ago (6), 87 the potential for this technique to improve hedonic appetite control has seen an increase in 88 published data. However, despite the promising effects outlined in this early study, more 89 recent data shows equivocal effects (7-10). This may be due to a lack of replication of data 90 as studies have employed varying designs (e.g., between- and within-group design), 91 outcome measures and stimulation parameters. The modulatory effects of tDCS are driven 92 largely by the specific stimulation parameters and device set-up (11). This includes the 93 electrode montage, current intensity and density, stimulation duration, and number of 94 sessions. Online protocols may also impact the modulatory effects (12). Despite the evident 95 variation caused by altering stimulation parameters, these parameters can vary greatly 96 between studies resulting in large variation in data (4, 13). This demonstrates the importance of identifying and consistently applying parameters that are known to modulate the outcome
measure. This is not a new concept (3, 12, 14), but has not been discussed in-depth for
studies measuring eating-related outcomes.

100

101 Understanding the ability of tDCS to modify eating behaviors is particularly difficult with 102 variation in study design, outcome measures and stimulation parameters. If indeed this 103 technique is to be used as an additional or adjunctive treatment modality for weight 104 management, it is important that these inconsistencies are addressed (15). Here we expand 105 on recent reviews (16, 17) to provide further detail on the potential impact of different 106 stimulation parameters and widen the discussion to incorporate important parameter 107 considerations, including reference electrode placement, electrode size, current density, 108 blinding efficacy, and the use of offline/online protocols. Specifically, we aim to identify 109 effective tDCS parameter ranges for the modulation of eating behavior, and determine 110 whether null effects are driven by parameters outside of these ranges.

111

#### 112 **2. METHODS**

#### 113 2.1. Search Strategy

114 An electronic literature search was performed in line with the Preferred Reporting Items for Systematic Reviews and Meta-Analyses (PRISMA) (18) (Table S1). The literature search 115 116 was completed using MEDLINE, PsycINFO and Scopus databases in March 2019, and 117 repeated in July 2020 to include additional articles published during this time. Search terms 118 are displayed in Table 1. An additional search was conducted using the Science Direct 119 database. Due to restrictions on Boolean terms and wildcards (\*), revised search terms were 120 used (Table 1). Results were limited to those written in English and published after 1998 to 121 coincide with the development of modern tDCS procedures (2, 19).

- 122
- 123

124

## \*\*\* INSERT TABLE 1 HERE \*\*\*

#### 125 2.2. Inclusion and Exclusion Criteria

126 After removing duplicates (n = 248), titles and abstracts were assessed for inclusion. Where 127 elimination based on title and abstract was not possible, full-text articles were retrieved and 128 assessed for inclusion in the final sample. Reviews, abstracts (where full-text articles were 129 unavailable), editorials/commentaries, book chapters, theses, study protocols, case reports 130 and animal studies were not included in the present review (total n = 68). Articles were 131 assessed in line with the Population, Intervention, Criteria and Outcome (PICO) model (20). 132 Articles were included if they were peer-reviewed intervention studies that recruited adult 133 human participants (population), applying conventional tDCS (i.e., one anode, one cathode) 134 procedures (intervention) which were sham-controlled (control), and reported an outcome 135 measure relating to eating behavior (food craving, food consumption, food reward, subjective 136 appetite) (outcome). Article selection was performed by two independent authors (JDB and 137 DS). Any further articles known to the authors were also considered for inclusion.

138

## 139 2.3. Data Extraction

For each eligible study, the following data were extracted: names of authors; year of publication; participant characteristics; montage and electrode size; current intensity and density; stimulation duration; ramp duration; sham protocol; number of sessions; blinding efficacy; use of online and offline protocols; outcome measures; main findings. Data were extracted as reported in the original article(s) by JDB.

145

#### 146 2.4. Study Quality Assessment

The quality of studies was determined using the Cochrane Collaboration's Risk of Bias (RoB) tool (21). Judgements were made by two independent authors at the study level; agreement between authors (JDB and NCS) was high ( $\kappa = 0.93$ ). This data will be used to identify issues with study design, particularly in relation to the delivery of tDCS.

151

## 152 2.5. Meta-Analysis

Means, standard deviations (SD) and sample size were extracted for eating-related 153 154 measures. Where standard error (SE) was reported, SD was estimated using the equation 155  $SD = SE \times \sqrt{n}$  (20). If data were not reported, datasets were requested from corresponding authors. Otherwise, means and SD or SE were extracted from available figures using 156 157 WebPlotDigitizer (version 4.4) (22), or estimated using the Practical Meta-Analysis Effect 158 Size Calculator (23) by entering t or F statistic and sample size. If data or effect sizes were 159 estimated, these were validated by two authors independently (JDB and NCS). Standardized mean differences were calculated and adjusted using Hedges' g due to small sample size (n 160 161 < 20) across many of the reviewed articles.

162

163 Analyses focused on single-session tDCS, to remove the potential cumulative effect of multi-164 session protocols. Four studies did not measure the effects of single-session tDCS and were 165 removed from analyses (24-27). Additional studies were removed due to missing data (28) 166 or due to all participants receiving active tDCS (29). To reduce confounding analyses, the 167 expectation effect observed by Ray et al. (30) was also removed. A total of 21 studies (n = 168 743 participants) were included in the meta-analysis (Table S5). Where possible, separate 169 analyses comparing single- versus multi-session tDCS were completed to identify any 170 cumulative effect (additional n = 3 studies, 105 participants). Where effect sizes are based 171 on composite scores (i.e., mean scores across varying levels of a specific parameter) within 172 the same participant group, these were removed from analyses for the specific parameter 173 measure to avoid confounding analyses (31, 32).

174

Differences in comparisons within experiments, journal articles, and research groups can
result in dependent effect sizes leading to narrow confidence intervals (CI) and small
estimates of SE (33, 34). We completed multilevel modelling to account for such
dependencies, with separate levels for comparisons within participant samples, experiments
within studies, and studies within the same research group. As indicated by Akaike

information criteria and likelihood ration test results, the addition of each level did notimprove model fit (Table S3).

182

183 Meta-analyses were performed using R (35) with the meta package (36). Due to the 184 variability in study design and outcomes, random effects models were used. Effect sizes 185 were interpreted as trivial (q < 0.20), small (q = 0.20), moderate (q = 0.50) or large (q > 0.80) 186 (37). A negative effect size favors active tDCS, indicating that active protocols reduce the 187 outcome measure. In comparison, positive effect sizes would indicate an increase in the 188 measure following active versus sham tDCS, favoring sham tDCS. Effect size heterogeneity 189 was assessed using the  $l^2$  index, and interpreted as might not be important (0 to 40%), may 190 represent moderate heterogeneity (30 to 60%), may represent substantial heterogeneity (50 191 to 90%), and may represent considerable heterogeneity (75 to 100%) (38). To test for 192 publication bias, Egger's regression was used (39). Subgroup analyses were conducted to 193 identify potential moderating effects of tDCS parameters on outcome measures. Where a 194 meta-analysis was not possible, a systematic literature review is included.

195

#### 196 **3. RESULTS**

197 In this section we provide the results of the review and discuss the findings. A total of 1,135 198 articles were identified, and after removing duplicates and assessing eligibility, 28 articles 199 were included in the present review (Figure S1). All reviewed studies used conventional 200 tDCS procedures and were sham-controlled trials, with 12 between-participant and 16 201 within-participant studies. A total of 996 participants were recruited across the reviewed 202 studies, ranging from 9 to 172 individuals per study, and included individuals with healthy 203 weight (n = 14 studies, 576 participants), overweight or obesity (n = 15 studies, 393 204 participants). Ljubisavljevic et al. (29) included individuals with healthy weight or overweight, 205 but do not provide total n for each weight category.

207 Most studies recruited individuals classed as "healthy", which refers to a lack of medical or 208 behavioral conditions and is irrespective of weight status. A small number of studies 209 recruited participants with specific conditions, such as Prader Willi Syndrome (40), Catechol-210 O-methyl transferase (COMT) Val158Met polymorphism (26, 27), frequent food cravings (6, 211 7, 41, 42), restrained eating (43, 44), binge eating disorder (45, 46), and anorexia or bulimia 212 nervosa (47, 48). Heterogeneity across studies ( $l^2$  range = 0 to 45%) suggests it might not 213 be important (Table S4). Funnel plots show good symmetry across measures (Figure S4), 214 with Egger's regression suggesting little evidence of publication bias (p > 0.08). A summary 215 of the meta-analytic data and forest plots are available in the Supplemental Digital Content.

216

## 217 3.1. Study Quality

218 Only 7 of the 28 studies showed low risk of bias across all domains, and therefore an overall 219 low risk of bias. Across the remaining studies, insufficient detail around participants and 220 researcher blinding was the greatest source of bias, particularly the process in which 221 researcher blinding was upheld. This also affected risk of bias judgement for the 222 measurement of outcome and selection of reported results. Most studies (n = 18) maintained 223 a double-blind protocol, either through the use of a pin-protected stimulation device or an 224 independent researcher completing stimulation protocols. Seven studies used a single-blind 225 design, with a further three studies providing insufficient detail around blinding protocols. 226

227 Additional bias arose due to the post-randomization exclusion of participants (n = 14 228 studies). Many studies do not provide a sample size calculation, which makes it difficult to 229 identify the impact of these exclusions. The exclusion of participants is particularly 230 problematic where this leads to a relatively small sample size, which is an important 231 consideration due to the repeated use of small sample size across tDCS research (14, 49, 232 50). Ray et al. (30) included a source of intended bias around participant blinding, with the 233 aim of assessing the impact of expecting to receive active versus sham tDCS on eating-234 related measures. Although this study received an overall high risk of bias, the study was

high-quality and this source of bias provides important considerations around the information
shared with participants. The RoB assessment is summarized in the Supplemental Digital
Content (Figures S2 and S3).

238

#### 239 3.2. Montage

240 The most common target location is the right dorsolateral prefrontal cortex (DLPFC) (n = 17), 241 with a smaller proportion of studies targeting the left DLPFC (n = 8) (Table 2). This cortical 242 region is of interest due to its role in executive functioning, a process associated with the 243 control of reward-driven appetite through the increase in inhibitory control and curbing of 244 impulsive behaviors (51, 52). Where the anode was placed over the right DLPFC and 245 cathode over the left DLPFC, a reduction across measures was seen (g = -0.39 to 0.01) 246 (Figures S5 to S10). Less consistent patterns were found when both anode and cathode 247 electrodes are placed over alternative cortical regions, although effect sizes are often based only on single studies (Figures S5 to S10; Table S2). The right DLPFC is of particular 248 249 interest as reduced activity of this region is associated with poor control of dietary behaviors 250 and obesity (53). The consistent negative effect sizes across eating-related measures when 251 targeting the right DLPFC may lend support for this right brain hypothesis of obesity (53).

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- 253

#### \*\* INSERT TABLE 2 HERE \*\*

254 255

256 Many studies delivering tDCS across other cortical regions also measured effects when 257 targeting the right DLPFC. Composite scores were calculated for these studies, to retain one 258 effect size per participant group and avoiding increasing homogeneity (31), and as such 259 were removed from analyses. However, the results of these studies provide further support 260 for targeting the right DLPFC. For example, Carvalho et al. (54) found increased preference 261 for chocolate following anode left/cathode right DLPFC stimulation, when compared with 262 both anode right/cathode left DLPFC and sham protocols. The authors also found craving intensity was reduced to a greater extent by anode right/cathode left montages compared
with anode left/cathode right DLPFC stimulation; replicating findings by Fregni et al. (6).

266 Further studies targeting the left DLPFC failed to identify a change in measures of subjective 267 appetite, food craving or food consumption (26, 27). Additionally, Marron et al. (55) found 268 increased hunger and desire to eat when applying 2.0 milliampere (mA) for 20 minutes with 269 the anode over the left DLPFC and cathode over the cerebellum. Targeting the left DLPFC 270 appears to have minimal effect on eating-related measures and suggests greater importance 271 for targeting the right versus left DLPFC, providing further support for the right brain 272 hypothesis (53). However, not all studies have found an effect of tDCS when applied to the 273 right DLPFC (Figures S5 to S10). This may be due to the eating behavior traits of the 274 recruited participants, with these studies recruiting individuals who do not display a 275 susceptibility to overconsumption and are likely able to appropriately inhibit impulsive 276 behaviors through effective executive control. In comparison, an effect is more consistently 277 shown in those with frequent food cravings or binge-type behaviors (6, 7, 41, 42, 45, 46). 278 This highlights a potential behavior trait-dependent effect of tDCS (56).

279

280 Novel target locations include the right inferior frontal gyrus (IFG) (43, 44), medial prefrontal 281 cortex (PFC) (48), right extrastriate body area (EBA) (48), and the primary motor cortex 282 representation of the tongue muscle (tnM1) (57) (Figure 1). These regions are additionally 283 associated with consumptive behaviors, however data following the use of these more novel 284 montages show no significant stimulation effects or an increase in measures of food 285 consumption and implicit preference (44, 48). The IFG and medial PFC are in anatomically 286 close proximity to the DLPFC, and the large electrodes used in these studies are likely to 287 overlap the DLPFC. However, these alternative montages likely change the current 288 distribution when compared to DLPFC-targeted stimulation (58). The effects of tDCS may be 289 dependent on the current entering the DLPFC, specifically the right hemisphere, and so the 290 small amount of current potentially entering through close proximity with an alternative target

| 291 | region may be insufficient to cause any meaningful modulation. This further suggests the          |
|-----|---|
| 292 | DLPFC is an important focal target for the modulation of eating behaviors.                        |
| 293 |   |
| 294 | ** INSERT FIGURE 1 HERE **  |
| 295 |   |
| 296 | In addition to variation in target location, researchers opt for different reference electrode    |
| 297 | locations. Across the included studies, the reference electrode was placed bilaterally to the     |
| 298 | target electrode (i.e., over the same cortical region, but on the opposite hemisphere; e.g.,      |
| 299 | right and left DLPFC), over the contralateral supraorbital region (i.e., above the eye on the     |
| 300 | opposite hemisphere; e.g., right DLPFC and left supraorbital region), or over the occipital       |
| 301 | lobe or cerebellum (Figure 1). A comparison of the potential effects of different reference       |
| 302 | electrode positions on eating behaviors has not been conducted, and it is difficult to fully      |
| 303 | identify any potential impacts. Moving the reference electrode to alternative locations is likely |
| 304 | to alter the current distribution, and may affect the expected tDCS-induced effects (58, 59).     |
| 305 | While there are similar reductions in eating-related measures when comparing tDCS with the        |
| 306 | same target location but differing reference electrode positions (e.g., left DLPFC versus left    |
| 307 | supraorbital region) (6, 7, 40-42, 45, 60), there was variation in effect sizes (Table S2).       |
| 308 | Again, these analyses should be interpreted with caution as the overall effect sizes are often    |
| 309 | based on single-studies and are likely driven by other variables.                                 |
| 310 |   |

311 One way to minimize the physiological impact of the reference electrode is to place it over an 312 extracephalic region, that is over a region of the body that is not the cortex (61). One study 313 placed the reference electrode over the contralateral cheek (43), and three studies placed 314 this electrode on a section of the participant's arm or shoulder (10, 29, 46). The advantage of 315 these extracephalic montages is that the physiological effects of the reference electrode are 316 minimized (62, 63), however this may be at the expense of altering the direction and 317 distribution of the electric current (14, 61). Despite these effects, placing the reference 318 electrode over an extracephalic region did not appear to impact the effects of tDCS on

behavioral measures as observed when using cephalic montages, with comparable effect
sizes following cephalic versus extracephalic montages (Table S2; Figures S11 to S16).

321

322

#### 323 **3.3.** Current Intensity and Current Density

324 The most consistently applied current intensity is 2.0 mA, delivered across 23 of the 28 325 studies. One study applied 1.5 mA (43), and 5 studies delivered 1.0 mA (9, 46, 48, 57, 60). It 326 has been suggested that 2.0 mA is the minimum intensity required to elicit changes in 327 eating-related measures (17, 32). However, since the publication of these papers, Chen et 328 al. (43) applied 1.5 mA and found improved reaction times in a stop-signal task. This 329 intensity warrants further investigation, especially in light of the potential issues surrounding 330 blinding efficacy at higher current intensities (64) (see 3.5). Unlike the earlier meta-analyses, 331 the present analysis found comparable effects of differing current intensities when 332 incorporating more recently published work (Figures S17 to S22).

333

334 It could be that, rather than current intensity, the effects of tDCS are driven more by the 335 density of applied current (i.e., the amount of current delivered per unit area [mA·cm<sup>-2</sup>]), as 336 low current densities will likely diminish the effect of stimulation on the underlying cortex (3). 337 The suggested minimum intensity of 2.0 mA equates to a minimum current density between 0.057 and 0.080 mA·cm<sup>-2</sup>, in line with commonly used electrode sizes of 25 and 35 cm<sup>2</sup>. 338 339 Indeed, this appears to be the boundary within which tDCS is able to modulate measures of eating behavior (Figures S23 to S28). In particular, 0.057 mA cm<sup>-2</sup> resulted in a consistent 340 341 reduction (i.e., favoring active tDCS) across all measures (g = -0.25 to -0.06). As 342 comparable current densities are achieved through varying current intensities and electrode 343 sizes, this may explain why we were unable to replication the intensity-dependent effect (17). 344

Maintaining a comparable current intensity, and therefore current density, does not occur in all studies. Four studies applied 1.0 mA using large 35 cm<sup>2</sup> electrodes, resulting in a current density of 0.029 mA·cm<sup>-2</sup> (9, 46, 57, 60). These studies failed to find an effect of stimulation
across measures of hunger and food craving, with the exception of Jauch-Chara et al. (60)
who identified reduced food consumption following repeated sessions of active tDCS,
potentially due to a cumulative effect (60) (see 3.7).

351

#### 352 3.4. Stimulation Duration

353 Stimulation was applied for 15 minutes (n = 1), 20 minutes (n = 23), 30 minutes (n = 3), and 354 40 minutes (n = 2) across the reviewed studies. Vicario et al. (57) delivered 15 minutes of 355 1.0 mA stimulation to the left tnM1, which failed to change subjective hunger scores. All 356 studies that used stimulation durations greater than 20 minutes also used multi-session 357 protocols, where tDCS was delivered over subsequent days (10, 25-27, 40) (see 3.7). 358 Comparison of effects following single-session tDCS as part of these multi-session designs 359 is largely not reported, and so the effects of longer stimulation durations in a single-session design cannot be made. Such extended durations should be used with caution, as data from 360 361 motor cortex stimulation suggests that longer durations may lead to a reversal of the 362 expected effect (65, 66). There are no recorded studies to date that have compared the 363 effects of stimulation duration on eating behavior outcomes, and further studies utilizing 364 shorter (10 to 15 minutes) durations are required as this would reduce the time requirement 365 of participants.

366

#### 367 3.5. Sham Protocols and Blinding

Commonly applied sham protocols involve the current being ramped up to the desired intensity and then delivered for 0 to 120 seconds before being ramped down (Figure 2). To imitate both the incremental and decremental currents integral to active tDCS protocols, some studies deliver the aforementioned ramping protocol at the start and end of the stimulation period. The common cutaneous sensations associated with delivery of the direct current typically occur at the start of current delivery (i.e., the ramp period) and often habituate within the initial seconds of stimulation (67). Therefore, sham protocols are considered effective methods of participant blinding as they mimic the initial phase of active
tDCS, but are unlikely to result in lasting modulation of the cortex due to the short duration
(67-69). Although standardized sham protocols are generally assumed to be effective,
researchers may struggle to maintain blinding at higher current strengths due to the more
pronounced cutaneous sensations (64).

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- 381

## \*\* INSERT FIGURE 2 HERE \*\*

382

383 Only 12 studies included quantitative data on the effectiveness of sham protocols, with 384 participants' ability to correctly guess the condition received ranging from 17 to 97% 385 (Cohen's d = 0.33 to 0.58). Of these studies, participants were unable to identify active 386 stimulation above the level of chance across 6 studies (9, 10, 29, 47, 54, 70). Many of these 387 studies utilized 2.0 mA, suggesting that participant blinding can be achieved at higher current strengths. Two further studies report successful participant blinding, but do not 388 389 provide data to support this (25, 42). The remaining studies reported failure to achieve 390 adequate participant blinding, with correct guesses ranging from 60 to 97% (7, 8, 43, 44, 46, 391 48). Again, these studies oppose the notion that higher current intensities result in poorer 392 participant blinding, as they include 1.0 and 1.5 mA protocols.

393

394 Based on the overall correct guess rate (i.e., number of participants able to identify active 395 and sham protocols), there are considerable differences in effect sizes when comparing 396 successful and unsuccessful blinding protocols. Where blinding was upheld, trivial-to-small 397 positive effect sizes were observed (g = 0.05 to 0.31) (Figures S29 to S34). In comparison, 398 studies with unsuccessful tDCS blinding resulted in more consistent negative effect sizes, 399 particularly across measures of explicit wanting, food craving and hunger (q = -0.16 to -0.11) 400 (Figures S29 to S34). Fassi and Cohen Kadosh (71) suggest, rather than focusing on overall 401 correct guess rate, we should instead assess active guess rate (i.e., percentage of 402 participants able to correctly guess receiving active protocols). The authors argue that

403 overall correct guess rate can lead to misleading estimate of blinding success (72). Across
404 the reviewed literature, overall correct guess rate suggests participant blinding may be
405 upheld (mean 48%, range 17 to 79%) whereas active guess rate demonstrates that
406 participants are consistently able to identify active protocols (mean 73%, range 60 to 85%).
407

In addition, the effects of researcher blinding cannot be ignored. When comparing the effects of single- and double-blind study designs on tDCS modulation of eating behavior, variation in effect sizes is evident (Figures S35 to S40). In particular, the reduction in food consumption and explicit wanting following tDCS appear to be driven by studies utilizing single-blind design. Discrepancy in effect sizes further emphasizes the importance of implementing and maintaining a double-blind study design.

414

#### 415 **3.6. Offline versus Online Protocols**

416 Offline protocols typically involve the participant remaining seated and relaxed with tDCS 417 delivered without distraction. In comparison, online protocols employ specific tasks during 418 the stimulation period, such as cognitive training (14). Many of the studies in this review 419 used offline protocols (n = 20). Eight studies applied online tDCS, where participants 420 watched unrelated media (e.g., nature documentary, cartoon) (10, 48), completed a food-421 related task (e.g., food choice computer-based task) (7, 9, 46, 73), or completed a cognitive 422 task (e.g., approach-avoidance training, Go/No-Go task) (8, 54). Variation in effect sizes is 423 evident when comparing offline and online protocols (Figures S41 to S46). Where offline 424 protocols produce a more consistent trivial-to-small negative effect size (g = -0.31 to 0.12), 425 with the exception of hunger measures, there is greater variation in the effects following 426 online protocols (g = -0.16 to 0.15).

427

#### 428 **3.7. Number of Stimulation Sessions**

A total of 9 studies included repeated sessions of active or sham tDCS, ranging from 3 to 16
 sessions. These multi-session studies appeared to result in a cumulative effect, with small

effect sizes for measures of food craving (g = -0.29; 95% CI = -0.60 to 0.03) and food consumption (g = -0.34; 95% CI = -1.03 to 0.35), compared to only trivial effect sizes following single session tDCS (g = -0.08 to 0.01) (Figure 3).

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- 435

# \*\* INSERT FIGURE 3 HERE \*\*

436

#### 437 **4. Discussion**

438 The findings of the review related to specifics of the studies and relevant parameters are 439 discussed above. In this section, we provide a general discussion of the findings with further 440 consideration of specific parameters. In this review we have considered the impact of a 441 range of stimulation parameters, and what methodological issues may explain the observed 442 inconsistencies in data. Figure 4 captures the variation in applied tDCS parameters across 443 the reviewed research. While our meta-analyses were unable to capture all parameter 444 variation, they have identified parameters that appear to modulate eating behavior. We 445 argue that a more holistic and comprehensive consideration of these parameters is required 446 to identify a consistent effect of tDCS protocols on eating-related measures. In Table 3 we 447 propose a range of tDCS parameters that appear to be most effective for modulating eating 448 behaviors. This is not intended as an absolute recommendation, but as a point of reference 449 and to help further discuss the most effective parameters for eating-related studies. In 450 addition to these, researchers should adhere to a double-blind protocol with a within-451 participant (randomized and counterbalanced) design, particularly for single-session studies 452 and where this fits the study aims. We also suggest that studies provide sufficient detail on 453 the study design and implemented tDCS parameters so the effects of parameter sets can be 454 fully understood. Protocols using parameters known to affect the outcome, such as online 455 tasks, should be carefully considered with a clear justification for their use.

- 456
- 457

458

## \*\* INSERT FIGURE 4 HERE \*\*

## \*\* INSERT TABLE 3 HERE \*\*

459

460 As discussed above, current density may be a more important driver of tDCS effects than 461 current intensity. Lower current intensities, such as 1.0 mA, can be utilized whilst maintaining 462 current densities in line with 2.0 mA protocols. For example, for 1.0 mA protocols the 463 electrode size can be reduced to between 12.5 and 17.5 cm<sup>2</sup>, resulting in current densities between 0.057 and 0.080 mA·cm<sup>-2</sup>. It should be noted that increasing the current density is 464 465 unlikely to lead to linear effects on the underlying cortex and outcome measures, but greater 466 current densities may provide more consistent effects (61, 74). Animal models suggest 467 tissue damage occurs at current densities above 25 mA·cm<sup>-2</sup> (75); to maintain participant 468 safety, current density should not exceed this threshold (76).

469

470 When considering the specific tDCS parameters, and the potential impact these may have 471 on behavior, the reference electrode should not be ignored as it is probable that this electrode exerts some physiological effect on the cortex which will likely affect outcome 472 473 measures (3, 58). Therefore, careful consideration of the placement of both electrodes is 474 required, with the reference electrode placed over a region unrelated to the outcome 475 measure (14). It is assumed that increasing the distance between electrodes results in a 476 greater amount of the current entering the brain, as opposed to being shunted across the 477 scalp (58). However, many studies place the target and reference electrodes relatively close together, such as bilaterally over the DLPFC (6, 7). 478

479

The effect of increasing electrode distance on measures of eating behavior is not clear. The ability of extracephalic montages to increase the amount of current penetrating deeper brain structures is also unclear (77, 78), although they do appear able to reduce the amount of current being shunted across the scalp (61, 79). If extracephalic montages are able to increase the amount of current reaching deeper brain structures, this may be important for reaching those structures involved in rewarding components of eating behavior, such as the nucleus accumbens (80). Further research that includes neuroimaging techniques is needed to support this premise. If an extracephalic montage is used, there should be careful
consideration of other parameters; for example, higher current intensities may be required to
compensate for the greater distance between electrodes (81).

490

491 Reflecting on the issues raised with reference electrode placement (see 3.20), any 492 modulatory effect of the reference electrode may be diminished by using a large electrode size. Electrodes are typically equal size of 25 or 35 cm<sup>2</sup>, but range from 16 to 70 cm<sup>2</sup>. When 493 494 electrodes are equal size there is similar cortical neuromodulation (with opposite polarity) 495 under both electrodes. In comparison, when the size of one electrode is increased, the 496 current density is reduced under that electrode which results in modulation under the smaller 497 electrode area only (82). Two studies have used larger reference electrodes (48, 70). 498 Although these studies do not show improvements in eating-related measures, this again 499 may be driven by methodological issues such as the use of an online task (48) (see 3.6). The use of large reference electrode size in eating behavior studies, especially with offline 500 501 protocols, is yet to be fully determined. Large reference electrodes can alter the current 502 distribution and may reduce the deleterious effects associated with the cathode (83). 503 Increasing reference electrode size should be combined with the use of greater distances 504 between electrodes, such as extracephalic montages, to minimize the chance of current 505 shunting across the scalp (79, 84).

506

507 The effects of tDCS are brain state-dependent and can be shaped by the use of online 508 protocols (3, 15). Offline protocols lead to modifications of cortical activity that last beyond 509 the stimulation duration, whereas the use of online tasks leads to modulation of cortical 510 activity related to the specific task (1, 85). Additionally, the use of an unrelated online task 511 may impact the expected polarity-dependent effects of tDCS (14). This may explain the lack 512 of expected effects on eating-related measures across the reviewed studies that use online 513 protocols. Even where a food-based training task is used to modify food choice behavior, 514 these studies typically measure wider eating-related measures such as food craving and

consumption (9, 73). Although food choice is an important driver of food consumption, food
cravings are a more influential predictor of dietary intake and focusing on tasks promoting
the regulation of food cravings may provide more fruitful effects (86)

518

519 It is currently unclear which participant populations may benefit from the use of online 520 protocols (74, 87, 88), and many studies fail to sufficiently justify the use of these protocols. 521 Where tDCS is delivered alongside a cognitive training task there appears to be improved 522 performance relating to the specific task, which highlights the importance of employing an 523 online task that is specific to the outcome measure of interest (88, 89). The impact of online 524 tasks on the direction of stimulation effects and outcome measures warrants careful 525 consideration of their use, but it may prove beneficial to use online protocols to enhance the 526 modulatory effects of tDCS on specific eating-related measures. However, the online tasks 527 performed in the reviewed studies are not always eating behavior-specific, and typically 528 focus on improving cognitive functions (8, 54). This may lead to improvements in the 529 cognitive measure, at the expense of improving eating behavior scores (85).

530

531 Gluck et al. (10) performed tDCS while participants watched nature or history documentaries 532 and they were able to show reduced consumption of fats and soda when comparing anodal 533 versus cathodal stimulation. This suggests the use of unrelated media with the aim diverting 534 thoughts away from food may prove a valuable procedure for standardizing participants' 535 thoughts during tDCS delivery. Until a clear effect of tDCS on eating behaviors is 536 consistently reported or a clear impact of online protocols on eating-related measures can be 537 identified, online protocols should be used with caution and a clear justification for their 538 inclusion should be provided.

539

Across the reviewed studies, stimulation was typically applied daily, with four studies initially applying stimulation with a 24-hour interval and increasing this to 48 hours in the second stage of the study (e.g., from inpatient to outpatient treatment) (24-27). Although a 48-hour 543 interval is likely to negate the cumulative effects of stimulation (90), it is possible that 544 increasing the interval to 48 hours following initial daily stimulation could strengthen the 545 modulatory effects. However, studies that implement this protocol failed to identify any 546 change in subjective appetite or food craving scores (24-27), but this may be due to their 547 focus on left DLPFC stimulation or longer stimulation durations. This poses an important 548 consideration for multi-session designs; whether daily sessions of stimulation are required, 549 or if the number of sessions can be reduced later in the study to minimize the time 550 requirements of participants. Again, further data are required to determine the impact of daily 551 to second-daily stimulation protocols, which should adhere to effective parameters.

552

553 There appears to be the potential for repeated session to negate the deleterious effects 554 when parameters are below the proposed effective range, as discussed in the above 555 sections. For example, Jauch-Chara et al. (60) used low current intensity (1.0 mA) and 556 density (0.029 mA  $\cdot$  cm<sup>-2</sup>), but they were able to demonstrate an ability of anodal tDCS to 557 reduce food consumption and subjective appetite following 8 sessions. This suggests that 558 repeated low-level stimulation may lead to a cumulative improvement in eating-related 559 measures, however there is not currently sufficient data to confirm this effect. If low-intensity 560 stimulation is able to modulate eating behaviors across multiple sessions, this may produce 561 a more consistent effect of tDCS than single-session stimulation but will require greater 562 resources and commitment from potential participants. Multi-session designs should not 563 come at the cost of appropriate stimulation parameters, and studies using single-session 564 stimulation are still important for determining effective parameter ranges and the modulatory 565 effect of tDCS on measures of eating behavior; they have also demonstrated significant 566 effects on a number of occasions (6, 7, 28, 45).

567

Reflecting on our RoB assessment, the implementation and maintenance of participant and
researcher blinding is the main source of bias across many of the reviewed studies. In
particular, little detail is given around researcher blinding protocols in several studies. It is

571 likely that poor researcher blinding contributes to poor participant blinding, as ineffective 572 researcher blinding can lead to several confounding factors such as expectation effects, 573 protocol adjustments or biases in the analysis and reporting of data (91). Researcher 574 blinding can be achieved through the use of pin-protected devices where the stimulation 575 parameters are pre-set by an independent individual (e.g., (70)). To control for potential 576 unblinding of researchers it is recommended that the efficacy of researcher blinding is 577 measured.

578

579 Additionally, the greater prevalence of adverse events following active tDCS may reduce the 580 ability to blind participants (92). However, this is of particular debate as not all studies find a 581 difference in adverse events between active and sham conditions (68). Poor blinding may be 582 driven by visual cues such as erythema (skin redness), which is more common following 583 active stimulation (64). This visual discrepancy between active and sham protocols easily 584 signifies to the participant and researcher that a difference between conditions exists and 585 potentially which condition the participant has received (64, 93). Six studies report either 586 greater erythema following active conditions or similar redness following active and sham 587 protocols (10, 24, 25, 40, 60, 70). Three of these studies reported successful participant 588 blinding, while also reporting no difference in skin redness (10, 25, 70), which suggests 589 erythema may indeed be contributing to ineffective participant blinding (64, 93).

590

Participant blinding can be maintained by preventing the participant from observing their skin following stimulation. However, researcher blinding is less straight forward to uphold where visible differences are evident and this may account for some of the variation in data (94). Careful consideration of stimulation parameters and device set-up should be made to minimize the likelihood of erythema and maintain a double-blind design. Additionally, pretreatment of the skin with dermatological products may reduce occurrence and severity of redness, but this may not be appropriate for all studies or participant groups (95). The impact 598 on current resistance by preparing the skin with these products is not well established, and 599 to account for any potential effects all preparatory steps must be recorded (11).

600

601 The information provided to participants should also be carefully controlled. Providing 602 information to participants that will lead to an expectation of effect will likely change scores, 603 resulting in an effect that is unrelated to the stimulation technique (30). Participants should 604 be given sufficient information to provide informed consent, but this should omit any study 605 hypotheses or expected effects of the study protocol. Answers provided to any participant 606 queries or comments made around the efficacy of tDCS should also be controlled. It should 607 be noted that individuals who have previously undergone or are knowledgeable of tDCS 608 procedures may be more likely to identify active protocols than tDCS-naïve individuals, and 609 so the inclusion of those who have previously undergone stimulation should be avoided to 610 maintain blinding efficacy (96).

611

612 Additional data are required to confirm some of the assumptions we have made, such as the 613 effective current density range, with further data required to determine the efficacy of some 614 parameters. We do not expect that all future studies will adhere to the parameters described 615 in this section, and it is important that further studies test the efficacy of parameters outside 616 these ranges. However, from the data included in this review, these appear to be the most 617 effective parameters for modulating eating-related outcomes. Whilst we acknowledge that 618 the present review does not extend to the discussion of physiological implications of differing 619 stimulation parameters, we have been able to describe those parameters that appear 620 effective on a behavioral level. The paucity of research describing the physiological effects of 621 tDCS remains problematic, ensuring it was not possible to fully discuss these implications in 622 this review. We encourage researchers to explore the physiological effects of differing tDCS 623 parameters to highlight the underpinning physiological mechanisms that drive the behavioral 624 effects we describe here.

#### 626 **5. CONCLUSION**

627 The first study measuring the effects of tDCS on food craving and consumption was 628 published more than a decade ago, and we are still at a relatively early stage in our 629 understanding of the effects and potential role of this technique for the control of eating 630 behavior. Interest in this area has proliferated over recent years, but many studies have 631 employed varying study designs and stimulation parameters which makes it difficult to 632 identify a consistent effect of tDCS. Careful consideration of stimulation parameters is 633 important for all studies. This is not a new concept with many recent reviews highlighting the 634 need for consistent and appropriate parameter use (3, 12, 14).

635

636 In this review, we have extended the discussion to incorporate a more comprehensive range 637 of parameters and have outlined potentially effective ranges for these parameters. We 638 acknowledge that some of the analyses, conclusions and assumptions we have made are 639 based on a limited number of studies, which reflects the relative novelty of these studies. 640 However, there is good evidence to support these conclusions from wider research, some of 641 which we have included in this review. Initial variation in applied parameters is important for 642 identifying the most appropriate parameters to apply. However, more consistency in 643 parameter application is required in future work in order to fully understand the impact of 644 tDCS and the efficacy of this technique to modulate the hedonic responses to food. This also highlights the need for publication of null effects and the use of Bayesian statistics, which 645 646 can be used to identify those parameters, populations or measures that appear to be outside 647 the modulatory influence of tDCS. The aim of this review was to identify effective parameter 648 ranges, and through our discussion we hope to improve the quality of future studies through 649 the application of appropriate study design and effective stimulation parameters. We also 650 hope this will also lead to continued discussion around these considerations.

651

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- 656

#### 657 AUTHOR CONTRIBUTIONS

- 658 Jordan D. Beaumont: Conceptualization, Methodology, Validation, Investigation, Data
- 659 curation, Writing original draft, Writing review & editing, Visualization, Project
- administration. **David Starr**: Validation, Data curation. **Natalie C. Smith**: Validation, Data
- 661 curation. **Danielle Davis**: Conceptualization, Writing review & editing, Supervision.
- 662 **Michelle Dalton**: Conceptualization, Writing review & editing, Supervision. **Alexander**
- 663 **Nowicky**: Writing review & editing. **Mark Russell**: Writing review & editing. **Martin J.**
- 664 **Barwood**: Conceptualization, Methodology, Validation, Writing review & editing,
- 665 Supervision.

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The critical role of cognitive-based trait differences in transcranial direct current stimulation (tDCS) suppression of food craving and eating in frank obesity. Appetite. 2017;116:568-74. 958 FIGURE CAPTIONS

959

960

- 961 **Figure 1** A comparison of cephalic montages; black circles represent target (left) or
- 962 reference (right) electrode locations. Image adapted from Klem, Lüders (97).
- 963
- 964 **Figure 2** A comparison between active and commonly applied sham protocols. In active
- 965 tDCS, the current is ramped up to the desired intensity and delivered for several minutes
- before being ramped down and switched off. Sham protocols involve the current being
- 967 ramped up to the desired intensity and then either immediately ramped down and turned off
- 968 (Sham A), or delivered for several seconds before being ramped down (Sham B).
- Alternatively, one of these sham protocols is repeated at the end of the stimulation period to
- 970 imitate both incremental and decremental currents integral to active tDCS protocols (Sham
- 971 C).
- 972
- 973 Figure 3 Forest plots comparing single- and multi-session protocol across (a) food craving974 and (b) food consumption measures.

975

976 **Figure 4** Summary of variation in tDCS parameters observed across the reviewed studies.

## **Table 1** Literature search terms

| Database                      | Search Terms  |
|-------------------------------|---|
| MEDLINE<br>PsycINFO<br>Scopus | ("noninvasive brain stimulation" OR "non-invasive brain stimulation" OR<br>"transcranial direct current stimulation" OR "transcranial current<br>stimulation" OR tDCS) AND (appetit* OR food OR "food crav*" OR<br>"food reward" OR "food preference*" OR "food cue" OR "food<br>consumption" OR eat* OR calorie* OR "calorie intake" OR "calorie<br>consumption" OR energy OR "energy intake" OR "energy consumption"<br>OR bing* OR "binge eat*" OR snack*) |
| Science Direct                | ("transcranial direct current stimulation" OR tDCS) AND ("food craving"<br>OR "food reward" OR "food preference" OR "food consumption")   |

# **Table 2** Comparison of tDCS parameters across studies

|                                     |                              | Monta                             | age <sup>a,b</sup>     | _                                    | Current           | Stin              | nulation Dura       | ition                      | - Number of             |
|-------------------------------------|------------------------------|-----------------------------------|------------------------|--------------------------------------|-------------------|-------------------|---------------------|----------------------------|-------------------------|
|                                     | Intervention                 | Target<br>Electrode               | Reference<br>Electrode | Electrode<br>Size (cm <sup>2</sup> ) | Intensity<br>(mA) | Ramp<br>(seconds) | Active<br>(minutes) | Sham<br>(seconds)          | Stimulation<br>Sessions |
| Amo Usanos<br>et al. (2020)<br>(24) | Anodal,<br>Sham              | F3                                | Right<br>supraorbital  | 25                                   | 2.0               | 30                | 20                  | 15 at start<br>and end     | 8                       |
| Beaumont et<br>al. (2021) (70)      | Anodal,<br>Sham              | F4                                | Oz                     | 25 / 51 °                            | 2.0               | 30                | 20                  | 36                         | 1                       |
| Bravo et al.<br>(2016) (40)         | Anodal,<br>Sham              | F4                                | Left<br>supraorbital   | 35                                   | 2.0               | 15                | 30                  | 0 (ramp<br>only)           | 5                       |
| Burgess et al.<br>(2016) (45)       | Anodal,<br>Sham              | F4                                | F3                     | Not reported                         | 2.0               | Not reported      | 20                  | 120 at start,<br>60 at end | 1                       |
| Carvalho et al.<br>(2019) (54)      | Anodal,<br>Cathodal,<br>Sham | F4                                | F3                     | 35                                   | 2.0               | 15                | 20                  | 15                         | 1                       |
| Chen et al.<br>(2019) (43)          | Anodal,<br>Sham              | Right IFG<br>(midpoint F4-<br>F8) | Left cheek             | 25                                   | 1.5               | 30                | 20                  | 0 (ramp<br>only)           | 1                       |
| Fassini et al.<br>(2019) (27)       | Anodal,<br>Sham              | F3                                | Right<br>supraorbital  | 25                                   | 2.0               | 30                | 30                  | 30                         | 16                      |
| Fassini et al.<br>(2020) (26)       | Anodal,<br>Sham              | F3                                | Right<br>supraorbital  | 25                                   | 2.0               | 30                | 30                  | 30                         | 16                      |

| Fregni et al.<br>(2008) (6)          | Anodal,<br>Cathodal,<br>Sham | F3 / F4     | F4 / F3                                 | 35           | 2.0 | Not reported | 20 | 30               | 1  |
|--------------------------------------|------------------------------|-------------|---|--------------|-----|--------------|----|------------------|----|
| Georgii et al.<br>(2017) (9)         | Anodal,<br>Sham              | F4          | F3                                      | 35           | 1.0 | 15           | 20 | 15               | 1  |
| Gluck et al.<br>(2015) (10)          | Anodal,<br>Cathodal,<br>Sham | F3          | Left forearm<br>/ Right<br>supraorbital | 25           | 2.0 | 30           | 40 | 15               | 3  |
| Goldman et al.<br>(2011) (7)         | Anodal,<br>Sham              | F4          | F3                                      | Not reported | 2.0 | 30           | 20 | 60               | 1  |
| Grundeis et al.<br>(2017) (73)       | Anodal,<br>Cathodal,<br>Sham | F8          | Af7                                     | 35           | 2.0 | 30           | 20 | 0 (ramp<br>only) | 1  |
| Heinitz et al.<br>(2017) (25)        | Anodal,<br>Sham              | F3          | Right<br>supraorbital                   | 35           | 2.0 | Not reported | 40 | 10               | 15 |
| Jauch-Chara<br>et al. (2014)<br>(60) | Anodal,<br>Sham              | Right DLPFC | Left<br>supraorbital                    | 35           | 1.0 | 8            | 20 | 0 (ramp<br>only) | 8  |
| Kekic et al.<br>(2014) (42)          | Anodal,<br>Sham              | F4          | F3                                      | 25           | 2.0 | 10           | 20 | 30               | 1  |
| Kekic et al.<br>(2017) (47)          | Anodal,<br>Cathodal,<br>Sham | F4          | F3                                      | 25           | 2.0 | 10           | 20 | 30               | 1  |

| Lapenta et al.<br>(2014) (41)           | Anodal,<br>Sham | F4                                | F3                     | 35        | 2.0       | 15           | 20 | 30                        | 1            |
|---|-----------------|-----------------------------------|------------------------|-----------|-----------|--------------|----|---------------------------|--------------|
| Ljubisavljevic<br>et al. (2016)<br>(29) | Anodal,<br>Sham | F4                                | Left forearm           | 35        | 2.0       | 30           | 20 | 0 (ramp<br>only)          | 5            |
| Marron et al.<br>(2019) (55)            | Anodal,<br>Sham | F3                                | Right<br>cerebellum    | 25        | 2.0       | Not reported | 20 | Not reported              | 1            |
| Mattavelli et<br>al. (2019) (48)        | Anodal,<br>Sham | Midpoint Fz-<br>F3 / O2-PO8       |                        | 16 / 35 ° | 1.0       | 10           | 20 | 40 at start,<br>30 at end | 1            |
| Max et al.<br>(2020) (46)               | Anodal,<br>Sham | F4                                | Left deltoid<br>muscle | 35        | 1.0 / 2.0 | 5            | 20 | 46                        | 1            |
| Montenegro et<br>al. (2012) (28)        | Anodal,<br>Sham | F3                                | Fp2                    | 35        | 2.0       | Not reported | 20 | 30                        | 1            |
| Ray et al.<br>(2017) (98)               | Anodal,<br>Sham | F4                                | F3                     | 24        | 2.0       | Not reported | 20 | Not reported              | Not reported |
| Ray et al.<br>(2019) (30)               | Anodal,<br>Sham | F4                                | F3                     | 24        | 2.0       | Not reported | 20 | 60 at start<br>and end    | Not reported |
| Sedgmond et<br>al. (2019) (8)           | Anodal,<br>Sham | F4                                | F3                     | 35        | 2.0       | 10           | 20 | 30                        | 1            |
| To et al.<br>(2018) (44)                | Anodal,<br>Sham | Right IFG<br>(midpoint F4-<br>F8) | Midpoint F3-<br>F7     | 25        | 2.0       | 30           | 20 | 0 (ramp<br>only)          | Not reported |

| (Table 2 | continued) |
|----------|------------|
|----------|------------|

| Vicario et al. | Anodal,   | Left tnM1 | Right   | 35 | 1.0 | 30 | 15 | 0 (ramp | 1 |
|----------------|-----------|-----------|---------|----|-----|----|----|---------|---|
| (2020) (57)    | Cathodal, |           | mastoid |    |     |    |    | only)   |   |
|                | Sham      |           | process |    |     |    |    |         |   |

Af7, anterior frontal area 7; DLPFC, dorsolateral prefrontal cortex; F3, frontal area 3; F4, frontal area 4; F7, frontal area 7; F8, frontal area 8;

Fp2, fronto-polar area 2; Fz, frontal zero point; IFG, inferior frontal gyrus; mA, milliampere; O2, occipital area 2; Oz, occipital zero point; PO2,

parieto-occipital area 2; tnM1, area of primary motor cortex representing the tongue muscle

<sup>a</sup> See Klem et al. (1999) (97).

<sup>b</sup> All sham protocols used the same montage as active protocols.

<sup>c</sup> Target electrode size / reference electrode size

## **Table 3** Proposed Effective tDCS Parameters

| Montage                      | Target: Right DLPFC<br>Reference: Cortical region away from DLPFC, or extracephalic region                                     |
|------------------------------|--|
| Electrode Size               | Target: ≤35 cm²<br>Reference: Equal or greater than target electrode   |
| Current Intensity            | 1.5 – 2.0 mA   |
| Current Density              | 0.057 – 0.080 mA⋅cm <sup>-2</sup>  |
| Stimulation<br>Duration      | 20 minutes   |
| Inter-session<br>Interval    | Single-session: >48 hours<br>Multi-session: ≤24 hours  |
| Offline / Online<br>Protocol | Offline; Unrelated media used as an online task may be appropriate for standardizing participants' thoughts during stimulation |
|                              |  |

| 984  | Supplemental Digital Content  |
|------|---|
| 985  |   |
| 986  |   |
| 987  | Table S1 PRISMA checklist.  |
| 988  |   |
| 989  | Table S2         Summary of meta-analytic data.   |
| 990  |   |
| 991  | Table S3 Output of multi-level modelling.   |
| 992  |   |
| 993  | Table S4         Summary of heterogeneity and publication bias data across eating-related |
| 994  | measures.   |
| 995  |   |
| 996  | Figure S1 PRISMA flow diagram detailing the search and selection process performed to     |
| 997  | identify studies applying tDCS for the modulation of eating behaviors.                    |
| 998  |   |
| 999  | Figure S2 Overall risk of bias across the 28 reviewed studies.                            |
| 1000 |   |
| 1001 | Figure S3 Risk of bias assessment within studies.   |
| 1002 |   |
| 1003 | Figure S4 Contour-enhanced funnel plots across eating-related measures.                   |
| 1004 |   |
| 1005 | Figures S5 to S10 Forest plots comparing montages.  |
| 1006 |   |
| 1007 | Figures S11 to S16 Forest plots comparing cephalic versus extracephalic montages.         |
| 1008 |   |
| 1009 | Figures S17 to S22 Forest plots comparing current intensities.                            |
| 1010 |   |
| 1011 | Figures S23 to S28 Forest plots comparing current densities.                              |

- **Figures S29 to S34** Forest plots comparing blinding success.
- **Figures S35 to S40** Forest plots comparing single- versus double-blind protocols.
- **Figures S41 to S46** Forest plots comparing online versus offline protocols.