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6 *The Way You Make Me Feel*: Psychological and Cerebral Responses to Music

7 During Real-Life Physical Activity

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## 29 Abstract

30 *Background:* The brain mechanisms that underlie the psychological effects of auditory  
31 stimuli during physical activity are hitherto under-researched; particularly so in ecologically  
32 valid settings. The objective of the present experiment was to investigate the effects of two  
33 contrasting auditory stimuli conditions on psychological responses and brain activity during  
34 an outdoor walking task.

35 *Methods:* Twenty-four participants were required to walk 400 m at a pace of their choosing  
36 and report perceptual (state attention and perceived exertion) and affective (valence, arousal,  
37 and perceived enjoyment) outcomes immediately after each exercise bout. Three conditions  
38 were administered in a randomised and fully counterbalanced order (control, podcast, and  
39 music). State-of-the-art, portable EEG technology was used to facilitate measurement during  
40 the walking task. Fast Fourier Transform was used to decompose the brain's electrical  
41 activity into different band waves (lower-alpha, upper-alpha, sensorimotor rhythm, and beta).

42 *Results:* The results indicated that music up-regulated beta waves, led to more dissociative  
43 thoughts, induced more positive affective responses, up-regulated arousal, and enhanced  
44 perceived enjoyment to a greater degree when compared to control and podcast.

45 *Conclusions:* Rearrangement of beta frequencies in the brain appears to elicit a more positive  
46 emotional state wherein participants are more likely to dissociate from internal sensory  
47 signals and focus on task-irrelevant factors. The portable EEG system used in the present  
48 study appears to accurately measure electrical activity in the brain during light-intensity  
49 physical activities and is effective in reducing electrical artefacts caused by body and cable  
50 movements.

51 *Keywords:* affect, arousal, attention, brain, motor activity, psychophysiology



77 Karageorghis, & Ekkekakis, 2014; Stork, Kwan, Gibala, & Martin Ginis, 2015). In the long  
78 term, pleasant sensory stimuli are hypothesised to increase adherence to physical activity  
79 programmes, which appears to be an effective strategy to reduce sedentariness and enhance  
80 well-being (Karageorghis & Priest, 2012a, 2012b; Priest & Karageorghis, 2008).

81         The brain mechanisms that underlie the effects of auditory stimuli during the  
82 execution of movements have only been investigated recently (Bigliassi et al., 2016a).  
83 Researchers have conducted laboratory-based experimental work to further understanding of  
84 the functional and cerebral mechanisms that underlie the effects of music during exercise  
85 (Bigliassi, Karageorghis, Nowicky, Orgs, & Wright, 2016a); which has been found to be an  
86 effective form of auditory stimulation. In the aforementioned study, participants were asked  
87 to execute a highly fatiguing isometric ankle-dorsiflexion type of contraction to the point of  
88 volitional exhaustion. The results indicated that the spectral power of low-frequency  
89 components (i.e., theta waves [4–7 Hz]) at the frontal, central, and parietal regions of the  
90 cortex were down-regulated when participants exercised in the presence of music.  
91 Interestingly, the same effect was not evident when participants listened to music at rest.  
92 Ostensibly, high-intensity exercise has the tendency to up-regulate theta waves, and music-  
93 related interventions appear to moderate this tendency.

94         It has been hypothesised that low-frequency components typically up-regulate as a  
95 means by which to induce a resting state (i.e., an index of neural fatigue; Craig, Tran,  
96 Wijesuriya, & Nguyen, 2012). Thus, pleasant auditory stimuli appear to engender a  
97 prophylactic effect (e.g., Boutcher & Trenske, 1990), in terms of potentially unpleasant  
98 psychophysical and affective responses, by rearranging the brain's electrical activity. Allied  
99 to this, music guides attention towards task-unrelated thoughts and reduces processing of  
100 internal sensory signals (e.g., muscle afferents). This psychophysiological mechanism is  
101 objectively indicated by reductions in the spectral power of theta waves (Bigliassi et al.,

102 2016a). Interestingly, individuals primarily execute whole-body movements at a light  
103 intensity during their daily physical activity routines (e.g., walking or cycling). In such  
104 instances, the effects of music-related interventions are primarily related to emotional  
105 experiences elicited by the stimuli (e.g., feeling happy; Koelsch, 2010; North, Hargreaves, &  
106 Hargreaves, 2004). Despite the fact that music has the potential to ameliorate fatigue-related  
107 sensations when individuals exercise at a light-to-moderate intensity, people tend to use it  
108 primarily as a means by which to render the exercise experience more pleasurable (Clark,  
109 Baker, & Taylor, 2016; Hallett & Lamont, 2015).

110         The brain mechanisms that underlie the effects of auditory stimuli on  
111 psychophysiological responses during the execution of lifestyle physical activity (e.g.,  
112 outdoor walking performed at light-intensity) have yet to be explored. Assessment of brain  
113 function has always proven to be a challenge in naturalistic settings given that cables and  
114 body movements tend to compromise the fidelity of the biological data. Fortunately, with  
115 advances in technology, researchers are now able to investigate electrical activity in the brain  
116 during real-life situations such as walking and cycling. For instance, portable EEG devices  
117 have recently been developed to facilitate the acquisition of biological data during physical  
118 activity. Such devices incorporate an electrical system that protects the core components of  
119 cables with active shielding technology. Specifically, this functions as a portable Faraday  
120 cage that prevents extraneous factors (e.g., cable movements) from interfering with the  
121 electroencephalographic signal (i.e., zero-capacitance). Accordingly, portable devices  
122 designed to measure electrocortical activity during the execution of gross movements can  
123 provide a direct and objective measure of an individual's emotional state and shine new light  
124 on the mechanisms that underlie the effects of environmental sensory stimuli on perceptual  
125 and affective responses.



## 151 **Experimental Procedures**

152 To further understanding of the psychophysiological mechanisms that underlie the use  
153 of music on physical activity, the present experiment employed a portable  
154 electroencephalography (EEG) system with active shielding technology. Participants engaged  
155 in singular bouts of light-intensity physical activity (walking) performed at self-paced speeds  
156 (i.e., real-life physical activity) on a standard all-weather 400-m running track. An additional  
157 auditory stimulus – a podcast – was used to facilitate identification of the effects of auditory  
158 distractions that are devoid of musical elements such as melody and harmony. The apparatus  
159 used in the present experiment was noninvasive and developed for use during the execution  
160 of movements. In total, the experimental procedures took no longer than 80 min.

161 **Pre-experimental phase.** Prior to engaging in the main experimental phase,  
162 participants were asked to read a participant information sheet, provide written informed  
163 consent, and respond to the Physical Activity Readiness Questionnaire (PAR-Q). The  
164 psychological measures to be used in the main phase were presented at this juncture as a  
165 means by which to improve participants' familiarity with them.

166 **Main-experimental phase.** A 32-channel EEG cap (EEGO Sports ANT Neuro) was  
167 placed on each participant's scalp, and conductive paste/gel (OneStep) was used to improve  
168 conductance between the biological signal and electrodes. The electronic devices were non-  
169 invasive and developed to be applied during movement (see Figure 1). Two experimental  
170 conditions (podcast [PO] and music [MU]) and a control (CO) were administered in a  
171 randomised and fully counterbalanced in order to identify the effects of auditory stimuli on  
172 electrical activity in the brain and psychological responses during exercise performed at light-  
173 intensities. A deterministic logarithm was used to randomise and counterbalance conditions;  
174 this was intended to prevent any influence of systematic order on the dependent variables. PO  
175 was used as a means by which to gauge the effects of auditory distractions that are devoid of



176 musical elements. Participants were required to complete 400 m in lane 1 of a running track  
177 at self-paced speeds and respond to psychological instruments (see Psychological measures  
178 section) immediately after the exercise bouts. The electrical activity in the right anterior  
179 tibialis was used to measure how long each participant took to complete the self-paced task.  
180 White noise (static sound) was used in between conditions as a *filler* to negate any potential  
181 residual effects of previous experimental conditions (León-Carrión et al., 2007).

182 \*\*\*Figure 1\*\*\*

### 183 **Auditory Stimuli Selection**

184 Music (MU): A 6-min version of *Happy* (160 bpm; Pharrell Williams; *Despicable Me*  
185 *2 soundtrack* album, 2013) was used as a means by which to guide the participant's  
186 attentional focus towards external influences and to enhance affective responses. Podcast  
187 (PO): *Building Better Cities* (TED Radio Hours) was selected as an auditory stimulus that is  
188 deemed to be task-irrelevant and neutral in terms of affective valence responses. PO was used  
189 in order to direct attention towards an auditory environmental cue that was devoid of musical  
190 properties during the exercise bout. The auditory stimuli were delivered via earphones (iPod  
191 compatible) and sound intensity was standardised at level 10, which is deemed relatively loud  
192 but entirely safe from an audiological perspective. A single-item auditory liking scale was  
193 used at the end of the experiment to gauge the degree to which participants liked the auditory  
194 stimuli (Karageorghis, Jones, & Stuart, 2008).

### 195 **Psychological Measures**

196 Four psychological measures were taken immediately after the exercise bouts.  
197 Attentional focus was assessed by use of a single-item attention scale (AS; Tammen, 1996).  
198 Affective valence was assessed by use of the Feeling Scale (FS; Hardy & Rejeski, 1989) Felt  
199 arousal was assessed by use of the Felt Arousal Scale (FAS; Svebak & Murgatroyd, 1985)  
200 Perceived exertion was assessed by use of Borg's single-item CR10 scale; Borg, 1982) The

201    aforementioned instruments were always administered in the same order (1st AS, 2nd FS, 3rd  
202    FAS, and 4th CR10). The Physical Activity Enjoyment Scale (PACES) was also administered  
203    at the end of each condition in order to assess the degree to which participants enjoyed each  
204    exercise bout.

### 205    **Electroencephalography**

206           Electrical activity in the brain was assessed throughout each exercise bout by use of a  
207    portable EEG system (see Figure 1). The core components of the EEG cables were protected  
208    with active-shielding technology, which served to reduce the influence of extraneous factors  
209    (e.g., cable movements) and body movements on the electrical signal. This technology was  
210    recently developed through the application of one layer of active shield that is used to  
211    receive, reflect, and reduce the electrical interference of signals at the frequency range of 50–  
212    60 Hz, and facilitate data collection in situations where a participant is physically active. The  
213    compact EEG amplifier was placed in a compatible and ergonomically-designed backpack  
214    where the signal was digitised at 500 Hz and analysed online. Thirty-two Ag/AgCl electrodes  
215    were attached to the participant’s scalp in accord with the guidelines detailed in the 10-20  
216    International System. The mastoid electrodes were used to digitally reference the electrical  
217    signal. Vertical eye movements were identified through the use of independent component  
218    analysis in order to remove the interference of eye blinks on frontal activity. The impedance  
219    level was kept below 10 k $\Omega$  and the signal was amplified at a gain of 1000 times. An online  
220    bandpass filter (0.1–100 Hz) was employed to reduce the influence of electrical artefacts on  
221    the acquired data.

222           The EEG signal was imported into the Brainstorm software (Tadel, Baillet, Mosher,  
223    Pantazis, & Leahy, 2011). Identification of bad electrodes and periods of electrical  
224    interference (bad segments) was the first procedure conducted to discard artefacts. A pair of  
225    electromyography (EMG) electrodes was placed on the participant’s right anterior tibialis in

226 accord with the recommendations of the SENIAM project (Surface Electromyography for the  
227 Non-Invasive Assessment of Muscles; Stegeman & Hermens, 1999). The EEG data were  
228 band-pass filtered offline (0.5–30 Hz), broken down into 1-s windows (asynchronous  
229 samples), and DC-offset corrected. One-second samples are representative of the time that  
230 most participants took to execute one step. Accordingly, changes in spectral power are more  
231 likely to represent the neural control of working muscles as well as the perceptual and  
232 affective changes associated with movement execution. The EMG activity indicated the  
233 period of time when the participant started and finished the test. The number of samples  
234 acquired in the present study ( $M = 215.4$ ,  $SD = 5.1$  samples) varied in accord with how long  
235 participants took to complete the self-paced task. The initial and final 15 s of activity were  
236 removed in order to reduce the influence of fast neurological adaptations to the initiation and  
237 cessation of movement. Fast Fourier Transform was used to decompose the brain's electrical  
238 activity into different brain frequencies. Lower-alpha (8–10 Hz), upper-alpha (10.5–12.5 Hz),  
239 sensorimotor rhythm (SMR; 13–15 Hz), and beta (15.5–29.5 Hz) waves were analysed to  
240 further understanding of the effects of auditory stimuli on the electrical activity in the brain  
241 during the execution of light-intensity bouts of physical activity (Bailey, Hall, Folger, &  
242 Miller, 2008; Enders et al., 2016).

243         The FFT values were acquired by averaging the spectra across samples. This option  
244 reduces the potential influence of waveform averaging as EEG signals were not time-locked  
245 to the gait cycle (Bigliassi et al., 2016a). The power spectrum was subsequently 1/f corrected  
246 (Tadel et al., 2011) given that power decreases with frequency (i.e., spectral flattening;  
247 multiplies the power at 8 Hz by 8). The frequency data were exported to Excel (Microsoft)  
248 for each electrode site and band frequency. Two-dimensional topographical results were used  
249 to illustrate the influence of different conditions on the brain's electrical activity grouped into  
250 predetermined band waves. The power spectra of five brain regions (Frontal: FpZ, Fp1, Fp2,

251 F3, F4, F7, and F8; Frontal-Central: FC1, FC2, FC5, and FC6; Central: Cz, C3, and C4;  
252 Central-Parietal: CP1, CP2, CP5, and CP6; Parietal: P3, P4, P7, and P8) were averaged and  
253 compared across conditions (Bigliassi et al., 2016b). Brainstorm (Tadel et al., 2011) was used  
254 to conduct the EEG procedures of the present study.

## 255 **Data Analysis**

256 Checks for univariate outliers were performed by use of standardised ( $z$ ) scores (i.e.,  $>$   
257  $3.29$  or  $< -3.29$ ) on IBM SPSS Statistics 22.0. The Shapiro-Wilk test was used to identify  
258 patterns of data distribution that do not fit the Gaussian curve. Log10 and square root  
259 transformations were computed in the case of non-normal profiles. Those variables that did  
260 not present a normal distribution after data correction were compared by use of  
261 corresponding non-parametric tests. The liking scores were compared using a paired-samples  
262  $t$  test. Task performance (i.e., time to complete the task), perceptual responses (i.e.,  
263 attentional focus and perceived exertion), affective responses (i.e., affective state and  
264 perceived activation), perceived enjoyment, and the time-averaged power spectrum for each  
265 predetermined brain region were compared across conditions by use of one-way repeated-  
266 measures analysis of variance (ANOVA). Bonferroni-adjusted pairwise comparisons were  
267 used to identify where differences lay. Friedman's analysis of variance by ranks was used for  
268 non-parametric data, followed up with the Wilcoxon rank tests to locate significant  
269 differences across conditions.

## 270 **Results**

271 No outliers were identified in the dataset but some variables did exhibit non-normal  
272 distribution. Accordingly, log10 transformations were used to normalise the distribution.  
273 Table 1 contains descriptive statistics for performance, perceptual, and affective variables.

274 The auditory stimuli (both CO and MU) used in the present experiment were  
275 considered to be moderately pleasant, and no significant differences were identified across

276 conditions ( $t(23) = 1.606; p = 0.122$ ). Additionally, task performance was not influenced by  
277 the presence of auditory stimuli ( $W = .642; \epsilon = .736; F(1.47, 33.86) = .54; p = .534; \eta_p^2 =$   
278  $.02$ ). Participants also reported similar exertional responses following execution of the task  
279 under the influence of PO and MU ( $W = .884; F(2, 46) = 2.61; p = .084; \eta_p^2 = .10$ ).  
280 Nonetheless, attentional focus was significantly influenced by the presence/absence of  
281 auditory stimuli ( $W = .996; F(2, 46) = 3.46; p = .040; \eta_p^2 = .13$ ). MU elicited more  
282 dissociative thoughts when compared to CO ( $p = .018$ ). No differences in attentional focus  
283 were identified between PO and MU ( $p = 0.251$ ) or CO and PO ( $p = .150$ ).

284 Participants' affective responses to exercise were also up-regulated during exercise in  
285 the presence of auditory stimuli ( $W = .951; F(2, 46) = 9.93; p < .001; \eta_p^2 = .30$ ). The piece of  
286 music used in the present study induced more positive affective responses than CO ( $p < .001$ )  
287 and PO ( $p = .029$ ). MU also up-regulated perceived activation to a greater degree when  
288 compared to CO and PO ( $p < .001$ ). Furthermore, perceived enjoyment was positively  
289 influenced by the presence of auditory stimuli ( $W = .764; F(2, 46) = 16.60; p < .001; \eta_p^2 =$   
290  $.42$ ) and this was associated with a large effect size. Bonferroni adjustments indicated that all  
291 conditions differed significantly from one another in terms of enjoyment (see Table 1).

292 \*\*\*Table 1\*\*\*

293 The results of the present study indicate that MU up-regulated high-frequency  
294 components of the power spectrum (i.e., beta waves) in the frontal (CO:  $M = 7.20, SD = 1.32;$   
295 PO:  $M = 7.21, SD = 1.31;$  MU:  $M = 9.23, SD = 1.59$  signal<sup>2</sup>/Hz\*10<sup>-10</sup>) and frontal-  
296 central (CO:  $M = 6.24, SD = 1.07;$  PO:  $M = 6.06, SD = 1.23;$  MU:  $M = 7.29, SD = 1.12$   
297 signal<sup>2</sup>/Hz\*10<sup>-10</sup>) regions of the brain to a greater extent when compared to CO and PO  
298 (see Table 2 and Figure 2).

299 \*\*\*Table 2\*\*\*

300 \*\*\*Figure 2\*\*\*

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## Discussion

The objective of the present study was to explore the cerebral mechanisms that underlie the effects of auditory stimuli in an ecologically valid setting and by use of portable EEG technology. The results indicate that music guided attention externally, induced more positive affective responses, up-regulated perceived activation, and enhanced perceived enjoyment to a greater degree when compared to CO and PO. Contrastingly, the podcast had no effect on perceptual and affective responses, but was sufficient to render perception of the task more pleasurable than CO (see Table 1). The brain mechanisms that underlie the effects of auditory stimuli on self-paced walking appear to be associated with the up-regulation of beta frequencies in the frontal and frontal-central regions of the cortex (see Figure 2).

The present experiment was designed to recreate a real-life scenario where participants could experience an everyday, outdoor physical activity; the EEG technology that was employed facilitated this. The exercise intensity was not expected to up-modulate exertional responses: we used self-paced walking to facilitate the processing of auditory stimuli and leave scope for participants to experience more dissociative thoughts (Hutchinson & Tenenbaum, 2007; Rejeski, 1985). In such instances, light-intensity exercises performed for short periods (~4 min) would have no detrimental effects on affective responses and cognitive processes (cf. teleoanticipation mechanism; Wittekind, Micklewright, & Beneke, 2011). However, participants reported different psychological responses in accord with the presence/absence of auditory stimuli, despite no differences in the physiological load induced in terms of exercise intensity. The present results appear to concur with similar findings, which show that music can render a given activity more pleasurable than under normal circumstances (see Hutchinson & Karageorghis, 2013; Karageorghis, 2016).

**326 Frequency of Cortical Rhythms**

327 Up-regulation of high-frequency waves in the frontal and frontal-central areas could  
328 be associated with the psychological benefits that are commonly induced by music during  
329 activities of daily life such as walking (Daly, Hallowell, et al., 2014; Daly, Malik, et al.,  
330 2014). Previous experiments have indicated that environmental sensory cues have the  
331 potential not only to up-regulate high-frequency components of the power spectrum, but also  
332 to downregulate theta waves in the frontal regions (Bigliassi et al., 2016b). Downregulation  
333 of low-frequency components have been associated with amelioration of fatigue-related  
334 symptoms such as limb discomfort during the execution of high-intensity exercise performed  
335 to the point of volitional exhaustion (Bigliassi et al., 2016a; Craig et al., 2012). On the other  
336 hand, high-frequency bands appear to change in response to one's level of activation  
337 (Aspinall, Mavros, Coyne, & Roe, 2015; Bigliassi et al., 2016b).

338 We hypothesise that increases in beta wave activity could be induced primarily by the  
339 arousal potential of a stimulus (Berlyne, 1971; Sayorwan et al., 2013). Up-regulation of high-  
340 frequency waves in the brain could also have a protective effect against fatigue-related  
341 sensations during highly-demanding motor tasks. In such instances, beta waves might have  
342 the potential to partially prevent the up-modulation of theta waves in the frontal cortex (i.e.,  
343 an inhibitory mechanism; Sherman et al., 2016), leading to a subsequent amelioration of  
344 fatigue (Bigliassi et al., 2016a; Craig et al., 2012; Tanaka et al., 2012). It is noteworthy that  
345 participants reported the task to be more enjoyable with the podcast when compared to CO,  
346 indicating that a calming and task-unrelated stimulus could maintain or even downregulate  
347 high-frequency waves and also render a given activity more pleasurable than under control  
348 conditions. Accordingly, future research is necessary to clarify the potential relationship  
349 between beta waves and psychological responses to exercise.

350

### 351 **Strengths and Limitations**

352           We selected auditory stimuli that would, in theory, elicit similar perceptual and  
353 affective responses across participants. Nonetheless, there is an idiosyncratic element to such  
354 responses (North et al., 2004). Despite the fact that both auditory stimuli were similar in  
355 terms of pleasantness, changes in how arousing the stimuli were perceived to be, could have  
356 induced changes in beta frequencies (Bigliassi et al., 2016b). Future research might employ  
357 the circumplex model of affect (Russell, 1980) and the associated affect grid (Russell, Weiss,  
358 & Mendelsohn, 1989) to further understanding of this potential confound prior to  
359 commencement of data collection. This is a means by which to standardise the emotional  
360 effects of the auditory stimuli (i.e., affective valence and arousal responses; North et al.,  
361 2004).

362           It is noteworthy that the differences in beta waves could have been induced by the  
363 sole effects of music regardless of the influence of exercise-related factors. Albeit previous  
364 research has indicated that such effects are not evident when participants listen to  
365 motivational pieces of music (see Bigliassi et al., 2016a), future studies might measure  
366 music-only effects on EEG activity as a means by which to further understanding of the  
367 combined effects of exercise and music on cerebral responses. Along similar lines, it is  
368 important to emphasise that one piece of music or even 10 pieces can never represent  
369 “music” as an artform in its entirety. Precisely the same principle applies to podcasts or  
370 audiobooks. The use of a wide range of musical selections/podcasts is not always viable in an  
371 experimental context given the high demands that this places upon participants. In this  
372 instance, we were primarily interested in the simple acoustic distinction of music *vs.* podcast,  
373 and are not claiming that our approach addresses the infinite complexity of such stimuli.

374           It is also important to emphasise that correlational analyses were not conducted in the  
375 present study given the differences in temporal resolution between EEG and the self-reported



376 measures. For example, changes in beta waves can be swift and marked during light-intensity  
377 exercise, while changes in affective valence can up-/down-regulate in a slower, more subtle  
378 manner. Therefore, the present authors can only speculate, based on previous findings (e.g.,  
379 Bailey et al., 2008; Sayorwan et al., 2013), that re-arrangement of beta waves in the frontal  
380 and frontal-central regions serves to up-/down-regulate affective responses.

381 Finally, it is important to note that we adopted a very prudent approach to process the  
382 data, and primarily focused our analyses on central areas of the cortex (e.g., frontal-central  
383 and central), avoiding the influence of electrical interferences caused by the leg and neck  
384 muscles. The device used in this experiment was purposefully designed to prevent noises  
385 generated by body and cable movements. It should be highlighted that walking tasks could  
386 have generated waves of electrical interference as a result of the impact of the heels on the  
387 track. Notably, the portable EEG technology employed in this study acquired meaningful  
388 electroencephalographic signals during the execution of gross movements performed at light-  
389 intensity and generally protected the core components of the cable against such electrical  
390 artefacts. Despite this, O1 and O2 electrode sites were affected by the electrical activity of the  
391 trapezius; such noises are not easily removed by use of traditional filtering methods (e.g.,  
392 band-pass filtering; Enders et al., 2016; Enders & Nigg, 2015; Kline, Huang, Snyder, &  
393 Ferris, 2015).

### 394 **Conclusions**

395 The present authors conclude that the psychological effects of music on low-intensity  
396 bouts of physical activity could be associated with the up-/down-regulation of high-frequency  
397 waves in the frontal and frontal-central regions of the brain. Rearrangement of beta  
398 frequencies in the brain appears to elicit a more positive emotional state where participants  
399 are more likely to dissociate from internal sensory signals and focus on task-irrelevant  
400 factors. This positive psychophysiological state induced by musical stimuli can be capitalised



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566 **Figure Captions**

567 *Figure 1.* Experimental set-up with the portable EEG technology.

568 *Figure 2.* Group data time-averaged band frequencies for CO, PO, and MU.

569 *Note.* SMR = Sensorimotor Rhythm. The coloured scale indicates the power of the band

570 frequencies ( $\text{signal}^2/\text{Hz} \cdot 10^{-10}$ ); CO = Control condition; PO = Podcast condition; MU

571 = Music condition; \* = MU was statistically different to both CO and PO ( $p < .05$ ).

572

\*\*\*Table 1\*\*\*

573 Table 1

574 *Descriptive Statistics for Liking, Performance, Perceptual, and Affective Variables*

	CO		PO		MU	
	<i>M</i>	<i>SE</i>	<i>M</i>	<i>SE</i>	<i>M</i>	<i>SE</i>
Liking Scores	–	–	6.33	.46	7.33	.45
Task Performance (s)	269.75	5.08	269.9	4.67	267.33	5.43
Attentional Focus	74.58	4.54	81.45	3.65	86.87	3.30
Perceived Exertion	1.68	.16	1.58	.13	1.39	.10
Affective Valence	3.25	.25	3.58	.25	4.08	.18
Perceived Activation	3.01	.27	2.85	.22	3.91	.30
Enjoyment	76.20	4.61	86.66	3.92	98.51	2.59

575 *Note.* CO = Control condition; PO = Podcast condition; MU = Music condition; *M* =  
 576 Mean; *SE* = Standard error.

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578

\*\*\*Table 2\*\*\*

579 Table 2

580 *One-way Repeated-Measures (RM) ANOVA Results for Time-Averaged Band*581 *Frequencies*

		Sphericity		RM ANOVA			
		<i>W</i>	$\epsilon$	<i>F</i>	<i>df</i>	<i>p</i>	$\eta_p^2$
Lower Alpha	Frontal	.93	.93	.94	2, 46	.398	.04
	Frontal-Central	.73	.79	.77	1.58, 36.46	.442	.03
	Central	.77	.81	.96	2, 46	.374	.04
	Central-Parietal	.86	.88	1.73	2, 46	.189	.07
	Parietal	.63	.73	1.79	1.46, 33.66	.188	.07
Upper Alpha	Frontal	.90	.91	.47	2, 46	.626	.02
	Frontal-Central	.82	.85	.75	2, 46	.478	.03
	Central	.94	.95	.28	2, 46	.754	.01
	Central-Parietal	.97	.97	.58	2, 46	.561	.02
	Parietal	.77	.81	1.27	2, 46	.289	.05
SMR	Frontal	.76	.81	.88	2, 46	.419	.03
	Frontal-Central	.78	.82	.43	2, 46	.653	.01
	Central	.93	.93	.46	2, 46	.631	.02
	Central-Parietal	.94	.94	.72	2, 46	.488	.03
	Parietal	.88	.89	1.51	2, 46	.231	.06
Beta	Frontal	.76	.80	3.32	2, 46	.045	.12
	Frontal-Central	.85	.87	3.25	2, 46	.048	.12
	Central	.87	.88	2.94	2, 46	.062	.11
	Central-Parietal	.94	.94	2.96	2, 46	.061	.11
	Parietal	.90	.91	2.97	2, 46	.061	.11

582 *Note.* SMR = Sensorimotor rhythm.

583

Figure 1

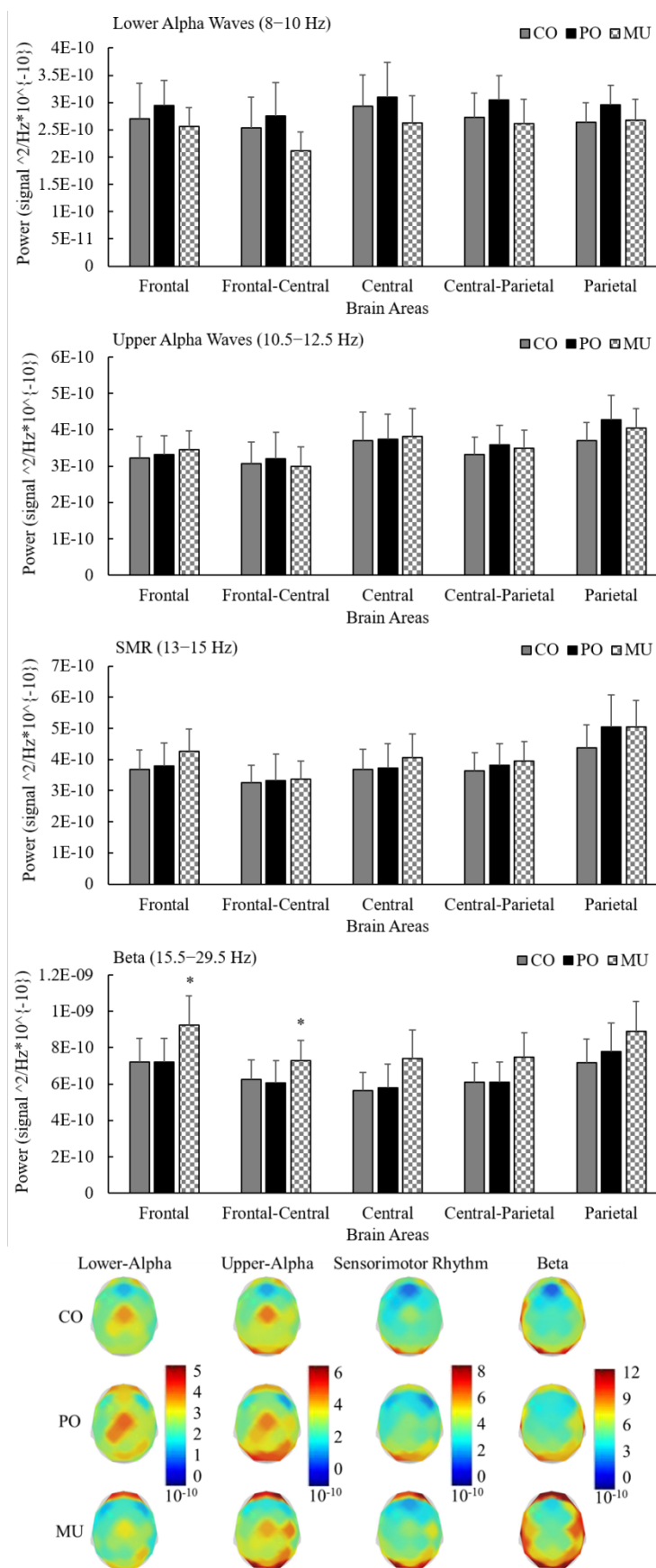


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Figure 2



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